

High cervical spinal cord stimulation: Effects on consciousness for minimally conscious patients.

Albert J Fenoy¹, Catarina Couras², Laura Barros³, Georgios Matis⁶, Serdar Baki Albayrak⁷, Aslihan Cevik⁸, Turker Karanci⁹, Ibrahim Halil Ural⁸, Arzu Dinc Yavas⁹, David Darrow³⁰, Igor A. Lavrov¹¹, Amit Kumar Tomar¹⁰, Therana Aliyeva³¹, Leyla Shahbazova³², Pritam Majumda^{33*}

¹Department of Neurosurgery, The University of Texas, Houston, USA

²Department of Neurology, University of São Paulo, SP, Brazil

³Department of Neurosurgery, Istanbul Aydin University, Istanbul Medical Park Florya, Turkey

⁴Department of Stereotactic and Functional Neurosurgery, University Cologne Hospital, Germany

⁵Department of Physical Medicine and Rehabilitation, Istanbul Aydin University, Istanbul Medical Park Florya, Istanbul, Turkey

⁶Department of Neurosurgery, University of Minnesota, Twin Cities, Minneapolis, Minnesota, USA

⁷Department of Neurology, Department of Biomedical Engineering, Mayo Clinic, Rochester, NY, USA

⁸Department of Neurology, Kazan Federal University, Kazan, Tatarstan, Russia

⁹Department of Anaesthesia and Neuromodulation, Indo-gulf Hospital, India

¹⁰Department of Medicine and Neurology, Bezmialem Vakif University, Istanbul, Turkey

¹¹Department of Neurology, Real Hospital, Baku, Azerbaijan

¹²Department of Functional Neurosurgery and Neuromodulation, Neuraxisdbs Care and research Centre India

¹³Department of Stereotactic and Functional Neurosurgery and Neuromodulation, University Cologne Hospital, Germany

Received: 30-May-2022, Manuscript No. AAJBN-22-65428; **Editor assigned:** 1-Jun-2022, AAJBN-22-65428 (PQ);

Reviewed: 15-Jun-2022, QC No. AAJBN-22-65428; **Revised:** 01-Aug-2022, Manuscript No. AAJBN-22-65428);

Published: 08-Aug-2022, DOI: 10.35841/AAJBN-5.5.121

Abstract

Background: The concept of Minimally Conscious condition or State (MCS) was proposed in the year 2002 and it is characterized by inconsistent but clearly discernible behavioural evidence of consciousness, which can be distinguished from coma and vegetative state by the presence of specific behavioural features not found in either of these conditions. Literary evidence exists for the usage of Deep Brain Stimulation (DBS) and High Cervical Spinal Cord Stimulation (HC-SCS) to restore consciousness for vegetative state and minimally conscious state patients.

Objective: The aim of this study is to determine: 1) Specific stimulation related neurophysiological responses in patients, such as Cerebral Blood Flow level (rCBF), auditory brain stem responses, somatosensory evoked potential responses, pain responses (related P-250 scaling), and electroencephalography responses. 2) Neuromuscular activity in upper extremities during stimulation by providing Electromyography (EMG) biofeedback data. 3) HC-SCS efficacy in spasticity level for brain injury patients using Modified Ashworth Scaling (MAS). 4) Post-stimulation therapy efficacy measure in combination with Bispectral Index Scoring (BIS). 5) Patient selection criteria for optimal therapy resulting in high cervical stimulation.

Materials and methods: Six patients with minimally consciousness condition were selected for this study. Eight electrode cylindrical leads were implanted at the C2-C6 level in six MCS patients followed by stimulation with 30 minute cycles (30 minutes 'ON' and 30 minutes 'OFF') for one year. Several

sets of electrode configurations, with variable amplitude, pulse width and frequency, were applied. For each combination, Cerebral Blood Flow (CBF), Electromyography (EMG) signals, Bispectral Index Scoring (BIS), auditory brainstem responses with Electroencephalography (EEG) as well as Modified Ashworth Scaling (MAS) for spasticity were measured and recorded.

Results: One week post-high cervical stimulation, an increment of CBF was observed in all six patients that correlated with an improvement of responses in the upper extremities. In all patients, the mean CBF without stimulation was 37.67 ± 1.91 ml/100 g/min, while at the 2nd week post-stimulation, the mean CBF was 49.31 ± 2.25 ml/100 g/min. The increment in post stimulation within 2nd week CBF level in these patients was observed to be approximately 12% ($p < 0.05$, paired t-test). There was a continuous improvement in the consciousness level as evident by the measured BIS value throughout the year and even after stimulation was stopped completely (post 52nd week).

Conclusions: HC-SCS therapy shows significant improvements in patients with MCS. Improvements were observed after terminating the stimulation after 12 months in 5 out of 6 patients. Such results are highly dependent on proper lead placement and optimal programming of the SCS device.

Keywords: Minimally Conscious State (MCS), Spinal Cord Stimulation (SCS), High Cervical Spinal Cord Stimulation (HC-SCS), Vegetative State (VS), Deep Brain Stimulation (DBS), Auditory Brainstem Responses (ABR), Somatosensory Evoked Potentials (SEP), Electro-encephalography (EEG).

Introduction

Disorder of consciousness is a state where normal brain functions like wakefulness and awareness have been affected by damage to part of the brain. Wakefulness is the ability to open and close eyes and demonstrate basic reflexes such as coughing and swallowing. Awareness is associated with more complex thought processing and performing more critical reflexes.

Before 1972, according to Jennet and Plum's definition, a wide range of characteristics were used to describe the different features of Vegetative State (VS), such as 'Apallic state', 'akinetetic mutism', or 'coma vigile'. Between 1972 and 1994, multiple task research bodies devoted significant effort towards a more precise definition of a condition of complete unawareness of the self and the environment accompanied by sleep-wake cycles with either complete or partial preservation of the brainstem autonomic functions [1-11]. Persistent VS (PVS) can result from various conditions but generally involves significant pathology within the cortex, subcortical white matter, and/or thalamus [4]. VS is a stage where patients are awake but have no signs of awareness. In VS, many patients open their eyes but do not show any meaningful responses such as following an object with their eyes or responding to voices. In VS, patients also do not show any emotional changes. Considering these facts, VS can be divided into two categories one, continuing vegetative state when it has been longer than 4 weeks and second, permanent vegetative state when it has been more than 6 months.

In 2002, Minimally Conscious condition or State (MCS) was proposed and it is characterized by inconsistent but clearly discernible behavioural evidence of consciousness [4-7]. MCS can be distinguished clearly from coma and VS by the presence of specific behavioural features, such as a patient who shows clear but minimal or inconsistent awareness and/or may have

periods where they respond to commands like moving a finger for a very minimum short time when asked [5]. Continual and/or permanent MCS is defined as MCS for >4 weeks; it is more difficult to diagnose because it depends on [1] the type of injury [2] the severity of the injury [3] responsiveness of the patient [5].

Multiple studies have reported that Deep Brain Stimulation (DBS) and Spinal Cord Stimulation (SCS) provide benefit to patients suffering from PVS and MCS by improving consciousness, but often lack precise characterization of baseline brain functions. Despite these advancements, no definitive trial or consistent guidelines have emerged for neuromodulation as a treatment of PVS, MCS, or AMCS; further studies are needed to provide evidence based clinical guidance [7-28]. Recently, one such study showed that SCS in the cervical region stimulated the Ascending Reticular Activating System (ARAS) causing increased awareness [3-31]. In another case SCS resulted in an improved clinical outcome in 2 out of 6 VS patients [2-6]. Another study showed a 54% improvement in regaining consciousness for MCS patients [12]. As reported by Yamamoto, 7 out of 10 MCS patients improved 70% after SCS therapy and those patients regained consistent functional interactions [1-32]. SCS has been found to enhance Cerebral Blood Flow (CBF) and cerebral glucose metabolism by regulating the sympathetic system [31]. In their study showed that CBF can increase by an average of about 22% after SCS [16].

In 1985, Hosubuchi reported that High Cervical Spinal Cord Stimulation (HC-SCS) induced significant cortical CBF increases, whereas thoracic level SCS did not show any CBF improvement [9]. Isono described improved CBF secondary to high cervical low frequency stimulation in large animal models, hypothesizing a role of specific spinal cord pathways which may contribute to increase CBF [16]. Patel et al. demonstrated that changes in CBF level varies with different

spinal cord stimulation settings and that central process are influenced by stimulation rather than modifying cervical sympathetic outflow [10]. Despite these studies, SCS for MCS patients' needs more clarification, such as better patient selection criteria, improved neurophysiologic characterizations to adequately scale and continuously measure progress post-implant. This study is designed to provide more concrete details on High Cervical Stimulation therapy and future directions 'The role of HC-SCS in restoring consciousness and overall clinical improvement in patients with MCS'.

Materials and Methods

Study subjects: This study was designed and approved by Neuraxisdb's care and research centre and Brazil institutions ethical committees; this study was reviewed by McGovern medical school neurosurgeons and committee, Mayo clinic team and Turkish institution medical park hospital committee. This study included 6 MCS patients aged from 26 to 70 years (mean 46±4 years who have undergone HC-SCS therapy. The causes for the MCS were: head injury (2 patients; ischemic stroke (2 patients; vascular intra-cerebral hematoma (2 patients).

Electrophysiological evaluation: These patients underwent electrophysiological evaluations and we used for Auditory Brainstem Responses (ABR, Somato-sensory Evoked Potentials (SEP, pain related P-250 scaling, Electroencephalography (EEG), and brain perfusion scan for cerebral blood flow (SPECT) [1,23]. For ABR evaluations and recordings, needle electrodes were placed on the earlobes, vertex (CZ and forehead (ground with a band pass filter (10 Hz-3 KHz. For SEP evaluations, the electrodes were placed over the primary cortical Somato-sensory regions on the head with the reference electrode being placed on the earlobe with a band pass filter (0.5 Hz-3 KHz. The pain related P250 was recorded in a form of train of electrical shocks to the finger pad from the response of the vertex region at random intervals [10]. These evaluations consisted of constant current pulses of 0.5 Ms duration which were applied at a repetition rate of 500 Hz for 60 Ms. these stimuli were given at that intensity which showed the withdrawal of flexion reflex. The band pass was in the range from 0.1-6000 Hz. EEG evaluations were recorded using a monopolar lead and electrodes were placed on the parietal, frontal areas and earlobes on both sides [1-23].

Surgical procedure and device placement: During SCS surgery, patients were placed in the prone position. Through an 18 gauge Tuohy needle, four contact SCS leads were inserted into the midline of the dorsal epidural space at the C6-C7 level under radiographic guidance. Implanted leads: all patients with 977A275-60 SCS (Medtronic Inc., Minneapolis, Minnesota, USA. The stimulation leads were connected to Implantable Pulse Generators (IPG: 6 patients with 97702 Prime Advanced. The IPGs were placed under the anterior chest wall (Figure 1 and 2).



Figure 1. The entry point of the spinal cord lead guided by 3D C-arm images. Percutaneously we inserted the lead at the C5-6 spinal segment area and pushed towards the C2 cervical segment.

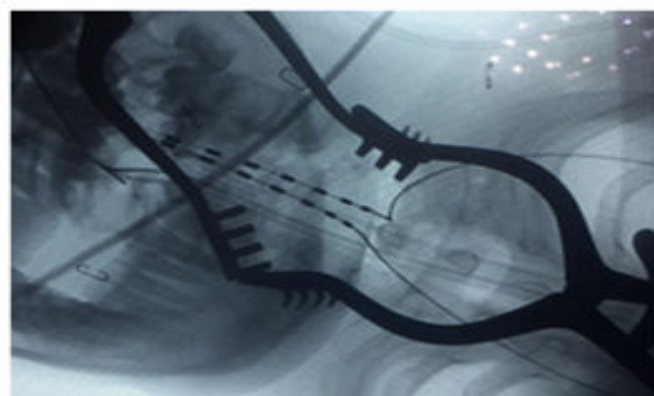


Figure 2. Shows final lead placement at C2 to C6 guided by 3D C-arm images.

Stimulation pattern: Postoperatively, 24 hour-stimulation started with a cyclic pattern of 30 minutes 'ON' and 30 minutes 'OFF' with Contact 0 as cathode and contact 3 as anode. Thus, effectively the patients were stimulated 12 hours/day. Different stimulation programming settings were implemented to determine the optimal stimulation parameters for each patient. We observed our patients post stimulation for seven days before changing the initial settings. Our stimulation parameters changed based on rCBF level and SMART assessment scaling to measure patients awareness level. SMART stands for Sensory Modality Assessment and Rehabilitation Technique; it is an assessment and treatment tool for use with patients who have profound brain damage. The SMART process takes about 14 weeks; this includes a 3-week initial assessment, 8 weeks of treatment, then a 3 weeks re-assessment. During SMART, specially trained assessors will look at the patient's responses to a variety of stimuli (sights, sounds, touch etc. and also see if the person is able to communicate in any way, or to participate in basic care tasks.

Detailed description of the programming parameters is described in (Table 1).

Table 1. Detailed description of the HC-SCS stimulation programming parameters with ON and OFF time for our 6 patients.

Electrodes combinations week basis programming settings.	OFF time ON time	Amplitude (V)	Pulse-width (µsec)	Frequency (HZ)
Contact-0 as Cathode, Contact-3 as Anode (1 st week-2 nd week).	30 mins ON 30 mins OFF	1.5 -2.5 V	270-300 µsec	20-30 Hz
Contact-0 as Cathode, Contact-3 as Anode (2 nd week-3 rd week).	30 mins ON 30 mins OFF	3.0-5.0 V	240-270 µsec	40-50 Hz
Contact-0 as Cathode, Contact-3 as Anode (3 rd week-4 th week).	30 mins ON 30 mins OFF	5.0-7.0 V	210-240 µsec	70-100 Hz
Contact-0 and 2 as Cathode, Contact-1 and 3 as Anode (4 th week-8 th week).	30 mins ON 30 mins OFF	1.5 -2.5 V	270-300 µsec	20-30 Hz
Contact-0 and 2 as Cathode, Contact-1 and 3 as Anode (8 th week -12 th week).	30 mins ON 30 mins OFF	3.0-5.0 V	240-270 µsec	40-50 Hz
Contact-0 and 2 as Cathode, Contact-1 and 3 as Anode (12 th week-32 nd week).	30 mins ON 30 mins OFF	5.0-7.0 V	210-240 µsec	70-100 Hz

Post-operative radiological measurements: Cerebral Blood Flow (CBF) was measured for all 6 patients. Single Photon Emission Computed Tomography (SPECT) was performed using the prism 2000 XP gamma camera system (Shimadzu Co. Kyoto). For CBF measurement, we used ethyl cysteinate dimmer to convert quantitative regional CBF (rCBF) images to qualitative axial SPECT images with the help of patlak plot graphical analysis with radionuclide angiography and lessen's linearization. Using this method, rCBF was estimated in the cortex, cerebellum and basal ganglia, first 2 days before high cervical stimulation and 7 days after high cervical stimulation 'ON' time. Changes in CBF in those brain regions with stimulation were measured in all MCS patients and were compared using the paired t-test [13-25].

Post-operative complete stimulation OFF: At one year post-implantation stimulation was turned OFF. During the year ON stimulation, we used different frequencies and different amplitudes and all patients were observed for this post-operative year and beyond according to patients' responses. CBF level was measured for each patient after one year of complete device OFF (Table 3).

Post-operative EMG biofeedback: Post operation, 6 out of 6 patients underwent advanced neurophysiological evaluation. All patients were evaluated by advanced EMG biofeedback systems to assess how EMG signals behave during stimulation ON time. This biofeedback system used surface electromyography for detecting responses from patient's active muscle movements using active bioelectrical signals when patients were able to respond to the verbal commands (e.g., 'move your hands', 'try to open fingers' and/or 'close hands' (Figures 3-7). Post-stimulation, 2nd week onwards, all patients were assessed based on EMG biofeedback system respectively.

Bispectral (BIS) value: The bispectral index monitor processes electroencephalographic signals to obtain a value, which reflects the level of consciousness of the patient. The consciousness data is displayed as a number (in a scale 0-100) on the BIS view monitor. A value of 0 represents the complete absence of brain activity, and 100 represent the maximum awake state. BIS values between 40 and 60 represent adequate general anaesthesia for a surgery; values less than 40 represent a deep hypnotic state. BIS value is usually maintained between 40 and 60 to prevent awareness. This study we used BIS monitoring for our all 6 MCS patients pre and post HC-SCS (Figure 8).

Post-operative changes in spasticity with stimulation: Patients with head injury (2 out of 6) had severe spasticity before HC-SCS as defined by the Modified Ashworth Scale (MAS), used this to measure stimulation improvements in spasticity. The Modified Ashworth Scale (MAS) measures resistance during passive soft-tissue stretching used as a simple measure of spasticity. Scoring taken from Bohannon and Smith:

- 0: No increase in muscle tone.
- 1: Slight increase in muscle tone, manifested by a catch and release or by minimal resistance at the end of the range of motion when the affected part(s) is moved in flexion or extension.
- 1+: Slight increase in muscle tone, manifested by a catch, followed by minimal resistance throughout the remainder (less than half) of the ROM.
- 2: More marked increase in muscle tone through most of the ROM, but affected part(s) easily moved.
- 3: Considerable increase in muscle tone, passive movement difficult.

- 4: Affected part(s) rigid in flexion or extension.

Criteria for determining emergences from MCS: We used two main criteria for determining the emergence from MCS:

- Functional interactive communication and ability to differentiate between two different objects; (SMART Assessment).
- Gestural or verbal (yes/no) responses and purposeful behaviour that is not associated with reflexive activity.

Results

Post-operative changes with stimulation: For the 6 patients in this study, the mean CBF without stimulation was

37.67±1.91 ml/100 g/min, while at 32 weeks post-stimulation, mean CBF was 49.31±2.25 ml/100 g/min. CBF level increased by an approximate 12% after stimulation ($p<0.05$, paired t-test) (Table 2).

Comparative study of CBF level of all patients

Table 2. Clinical features and post HC-SCS follow-up results (pre- and post- stimulation).

Case No.	Age (yrs.)	Cause of brain injury	Start of SCS After brain injury	CBF (ml/100 g/min)	
				Before HC-SCS	Post-32 nd -week during HC-SCS
1	32 (M)	Head Injury	5 months	42.35	52.87
2	26 (M)	Intra-cerebral hematoma	8 months	35.1	48.9
3	70 (M)	MCA infarct	7 months	37.98	47.1
4	58 (F)	MCA infarct	5 months	40.27	53.33
5	46 (M)	Head injury	6 months	38.19	50.9
6	66 (M)	Intra-cerebral hematoma	7 months	32.21	42.81

Post-operative EMG Signal changes during Stimulation: In the first few weeks post stimulation onset, EMG responses were negligible, as patients were not able to communicate and could not follow verbal commands. However, by post-operative 3-4 weeks, EMG biofeedback systems started showing responses. At 3 months post stimulation onset, patients' EMG biofeedback signals showed improved responses with increased muscle tone (Figure 3-7). Both upper and lower limbs' EMG biofeedback signals and graphs were analysed via EGZO tech device in supine as well as in sitting positions.

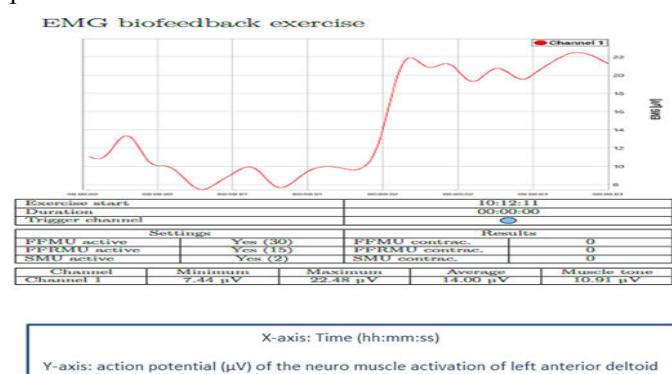


Figure 3. EMG biofeedback graph of our 1st patient while HC-SCS stimulation 'ON' using EGZO tech EMG Biofeedback system to determine muscle contraction when the patient was asked to move their hands, assessing whether verbal commands were being followed (3 weeks post- HC-SCS implantation).

This graph shows the patient started responding based on muscle contraction. Channel 1 electrode showed anterior deltoid contraction for left shoulder flexion and reference electrode placed on greater tubercle muscle. In this graph, it can be clearly seen that the initial electrode conduction was 7.44 microvolt but post stimulation reached 22.48 microvolt, muscle tone was 10.91 microvolt.

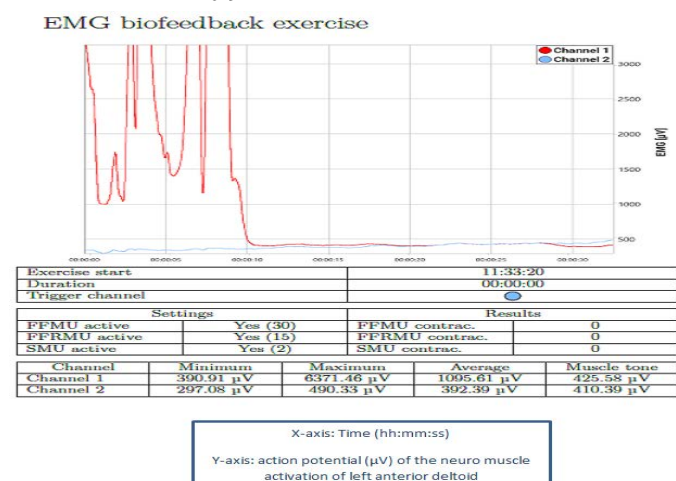
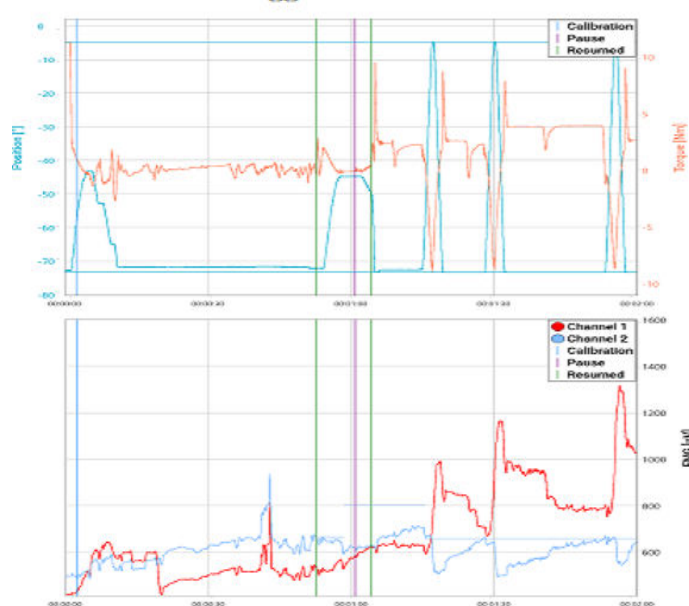


Figure 4. EMG biofeedback graph of our 1st patient while HC-SCS stimulation 'ON' using EGZO tech EMG Biofeedback system to determine muscle contraction when the patient was asked to move their hands, assessing whether verbal commands were being followed (12 weeks post HC-SCS implantation).

This graph shows the patient started responding based on muscle contraction. Channel 1 electrode showed anterior deltoid contraction for left shoulder flexion and reference electrode placed on greater tubercle muscle. Channel 2 electrode placed upon left biceps for elbow flexion and reference electrode placed upon medial epicondyle region. In this graph, it can be clearly seen channel 1 electrode conduction started with 390.91 microvolt and reached 6371.46 microvolt, whereas channel 2 electrode conduction started with 297.08 microvolt and went up to 490.33 microvolt. Muscle tone detected in channel 1 was 425.58 microvolt and in channel 2 was 410.39 microvolt.

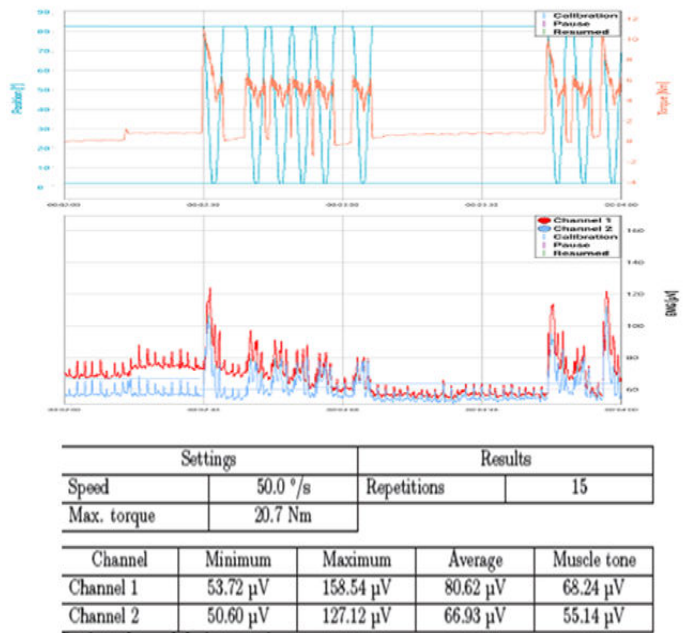
Reactive EMG Trigger & Release exercise



Settings		Results	
Speed	50.0 °/s → 38.7 °/s	Repetitions	4
Max. torque	17.3 Nm		
Channel	Minimum	Maximum	Average
Channel 1	414.67 µV	1493.99 µV	739.99 µV
Channel 2	411.25 µV	934.61 µV	594.76 µV

Figure 5. EMG biofeedback graph of our 2nd patient while HC-SCS stimulation ‘ON’ using EGZO tech EMG Biofeedback system to determine muscle contraction when the patient was asked to move their hands, assessing whether verbal commands were being followed (6 weeks post HC-SCS implantation).

This graph shows the patient started responding based on muscle contraction. Channel 1 electrode showed anterior deltoid contraction for right shoulder flexion and reference electrode placed on greater tubercle muscle. Channel 2 electrodes were placed upon left biceps for elbow flexion and reference electrode was placed upon medial epicondyle region. In this graph it is clearly seen channel 1 electrode conduction started at 414.67 microvolt and reached 1493.99 microvolt, where channel 2 electrode conduction started at 411.25 microvolt and went up to 934.25 microvolt. Muscle tone detected in channel 1 was 655.97 microvolt and in channel 2 was 582.37 microvolt.



Settings		Results	
Speed	50.0 °/s	Repetitions	15
Max. torque	20.7 Nm		
Channel	Minimum	Maximum	Average
Channel 1	53.72 µV	158.54 µV	80.62 µV
Channel 2	50.60 µV	127.12 µV	66.93 µV

Figure 6. EMG biofeedback graph of our 3rd patient while HC-SCS stimulation ‘ON’ using EGZO tech EMG Biofeedback system to determine muscle contraction when the patient was asked to move their hands, assessing whether verbal commands were being followed (3 weeks post HC-SCS implantation).

This graph shows the patient started responding based on muscle contraction. Channel 1 electrode showed anterior deltoid contraction for left shoulder flexion and reference electrode placed on greater tubercle muscle. Channel 2 electrodes were placed upon left biceps for elbow flexion and reference electrode was placed upon medial epicondyle region. In this graph it can be clearly seen that channel 1 electrode conduction started at 53.72 microvolt and reached 158.54 microvolt, where channel 2 electrode conduction started at 50.60 microvolt and went up to 127.12 microvolt. Muscle tone detected in channel 1 was 68.24 microvolt and in channel 2 was 55.14 microvolt.

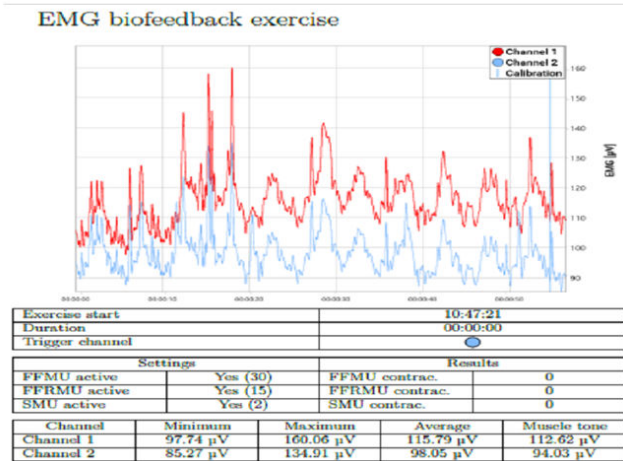


Figure 7. EMG biofeedback graph of our 3rd patient while HC-SCS stimulation 'ON' using EGZO tech EMG Biofeedback system to determine muscle contraction when the patient was asked to move their hands, assessing whether verbal commands were being followed (6 weeks post HC-SCS implantation).

This graph shows the patient started responding based on muscle contraction. Channel 1 electrode showed anterior deltoid contraction for left shoulder flexion and reference electrode placed on greater tubercle muscle. Channel 2 electrode was placed upon left biceps for elbow flexion and reference electrode placed upon medial epicondyle region. In this graph it can be clearly seen channel 1 electrode conduction started at 97.74 microvolt and reached 160.06 microvolt, where channel 2 electrode conduction started at 85.27 microvolt and went up to 134.91 microvolt. Muscle tone detected in channel 1 was 112.62 microvolt and in channel 2 was 94.03 microvolt.

Bispectral (BIS) value: Before HC-SCS stimulation, we measured all 6 patients' BIS score which ranged between 39-47. One week post HC-SCS the BIS score started to change

Table 3. Describes the CBF level post 1 year of the HC-SCS completely off condition. (*Case-1 did not respond well post device switched off, so we started the device once again).

Case no.	Before HC- SCS CBF (CBF(ml/100 g/min))	Post 1 year OFF HC-SCS CBF (CBF (ml/100 g/min))
2	35.1	55.01
3	37.98	62.84
4	40.27	59.97
5	38.19	60.87
6	32.21	49.64
1	42.35	46.87

ranging from 44-55 and continued for the 3rd week, 6th week and 12th week post-stimulation. At the 32nd week post-stimulation the BIS scoring ranged between 78-95 for all 6 patients. Interestingly, after a year we completely switched OFF the stimulation. At this new time point 1 year ON and 4 weeks OFF stimulation, the BIS score ranged between 85-95, a further improvement, implying patients had improved in their consciousness level. Details scoring given the BIS value graph in (Figure 8).

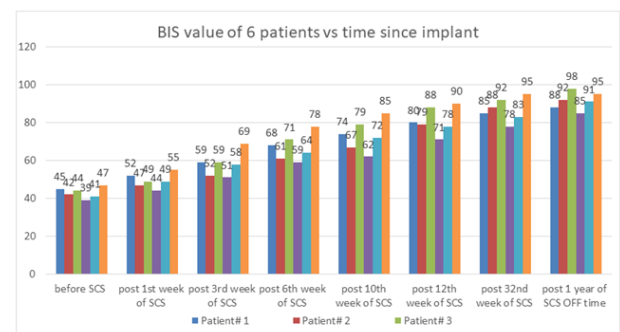


Figure 8. Describes 6 MCS patients before HC-SCS and after HC-SCS Bispectral value.

Post-operative 1 year stimulation completely OFF: For HC-SCS, the implant was performed at the C2-C6 region and stimulation was started post-implant. As mentioned earlier, for 1 patient the stimulation could not be stopped completely even after 12 months. We observed the remaining 5 patients up to 4 weeks after the device was completely switched OFF. Patients were observed to have sustained improvements with increased CBF levels (Table 3 and Figure 9). They were able to rotate a Rubik's cube and were able to communicate verbally with others.

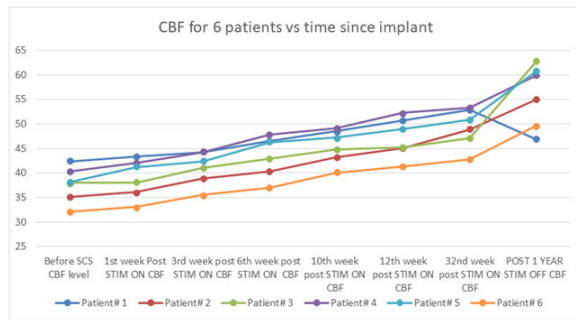


Figure 9. The CBF level of 6 patients from before HC-SCS implant (baseline) to 4 weeks after stimulation was stopped (Stimulation was ON for 52 weeks).

(*Case-1 did not respond well after post device switched off, so we started the device once again. This is also evident from the graph where the CBF dropped after stimulation was stopped).

Post stimulation spasticity: The HC-SCS helped 2 of our patients with brain injury, in terms of spasticity. At 1 month post-stimulation we began to observe rapid improvements in upper limb spasticity, whereas lower limbs had no significant change in spasticity throughout the stimulation. The details are shown in the graph (Figure 10).

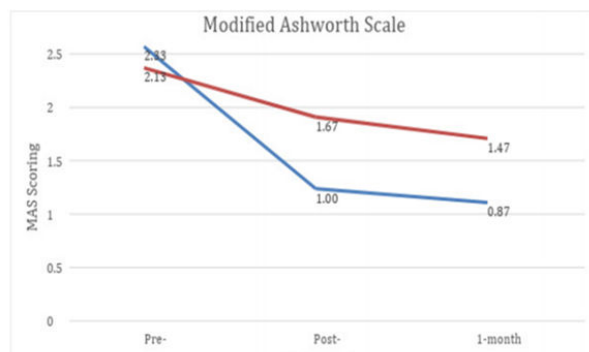


Figure 10. Plots the MAS level of 2 patients before HC-SCS implant (baseline) to 4 weeks after stimulation.

On the basis of these criteria, the 6 patients emerged from MCS following SCS therapy.

Case 1: A 32-year-old man suffered a road traffic accident. He sustained traumatic head injury leading him to a comatose state and a diagnosis of diffuse left cortical brain injury. Five months post injury, he was diagnosed with MCS. He was on a tracheostomy. He occasionally responded to physicians' orders by grasping hands but this was inconsistent. No other communication variations were observed during this period. He underwent HC-SCS therapy and was able to communicate consistently after 7 months of SCS stimulation. At 4 weeks post stimulation his tracheostomy was removed and he was able to breathe well through his mouth. After 1 year of stimulation, he was able to rotate the six planes of a Rubik's cube and was able to speak and communicate with others. He sufficiently overcame the upper motor dysfunction to complete

the Rubik's cube. However, lower limb recovery was unsatisfactory and he used a wheelchair for moving around.

Case 2: A 26-year-old man developed a left intra-cerebral hematoma because of severe hypertension. Initially the hematoma was removed to prevent impending herniation. Postoperatively, he remained in a MCS state for 8 months and was on a tracheostomy. During examination in hospital, he occasionally responded to verbal commands, such as grasping hands or closing his eyes. 4 months after HC-SCS onset, he was able to communicate consistently and his tracheostomy was removed at 6 weeks post-stimulation. Though he had left hemiparesis, he was still able to move his hands as per verbal commands. In terms of motor recovery, his upper extremity motor functionality improved and was sustained but his lower limbs never improved in motor strength. As a result, he required a wheelchair for moving around.

Case 3: A 70-year-old man having right Middle Cerebral Artery (MCA) infarction with right basilar involvement was in MCS for around 7 months with a tracheostomy. Before the cervical stimulation, the patient could follow some verbal commands. Very minimal functionality of the upper extremities was observed. Three weeks after the SCS implantation, the patient started following verbal commands consistently and the tracheostomy was removed. One month after stimulation, the patient followed all verbal commands with good upper limb extremities functionality (e.g., holding hands or holding fingers). Speech problems were unresolved and the lower limbs improvement was insufficient to walk, requiring a wheelchair mobilization.

Case 4: A 58-year-old female who had left Middle Cerebral Artery (MCA) infarction with left basilar involvement, was in MCS for around 5 months. Before the cervical stimulation, the patient could follow some verbal commands but not consistently. Very negligible functionality of the upper extremities was observed. Five weeks after the SCS implantation, the patient started following verbal commands consistently. Four months after stimulation, the patient followed all verbal commands with good upper limb extremities functionality (e.g., holding hands or holding fingers). Speech problems were unresolved and the lower limbs improvement was insufficient to walk.

Case 5: A 46-year-old man suffered a road traffic accident, with resultant head injury leading to a comatose state and a diagnosis of diffuse brain injury. Six months post injury; he was diagnosed with MCS with inconsistent responses to physicians' orders. He was on a tracheostomy. No other communication variations were observed during this period. He underwent HC-SCS therapy and he was able to communicate consistently 4 months after the initiation of SCS stimulation. Post stimulation 6th week, his tracheostomy was removed. After 1 year of stimulation, he was able to rotate the six planes of a Rubik's cube and he was able to speak and communicate with others. He sufficiently overcame upper motor functionality to complete the Rubik's cube as well as recover the lower limbs.

Case 6: A 66-year-old man developed an intracerebral hematoma. Initially the hematoma was removed to prevent forthcoming herniation. Postoperatively, he remained in MCS state for 7 months. In the hospital during examination time he obeyed occasional verbal commands, such as grasping hands or closing his eyes with tracheostomy. Five months after the HC-SCS, he was able to communicate consistently. Though he had right hemiparesis, he was able to use his hands to follow verbal commands. At 5 weeks post stimulation, his tracheostomy was removed. In terms of motor recovery, his upper extremity motor functionality improved and was sustained whereas his lower limbs improved less in motor strength, such that he required assistance to walk.

SMART assessment: In this study we have observed that our patients were able to rotate the six planes of a Rubik's cube and were able to speak and communicate with others at the end of the stimulation period (12 months). According to the Sensory Modality Assessment and Rehabilitation Technique (SMART), there are 5 different identifiable levels of consciousness. The five levels are no response (level 1), reflexive (level 2), withdrawal (level 3), localizing (level 4) and discriminating responses (level 5). This time frame and frequency of assessment is designed to provide frequent assessment over a short time frame to enable the assessor to establish if the behavioural responses observed are consistent and repeatable. A consistent response (on five consecutive assessments) at SMART (level 5) in any of the five sensory modalities, *i.e.* following verbal instructions, indicates a meaningful response. SMART provides the assessor with quantitative data of change over time through comparison of the SMART total scores. Considering this SMART assessment level scale, all patients reached a (level 5) on the SMART scale as they individually performed the rotation of Rubik's cube and were able to speak and communicate with others.

Discussion

In this work we report on 6 patients emerging from MCS due to HC-SCS therapy. Since 1980, only 15 articles have been published on the role of SCS in restoring consciousness, with the majority of them describing the magnitude of clinical improvement (restoration of interactions, ability to identify or speak); it is possible that in these cases VS was misdiagnosed or patient selections were done incorrectly. A few available observations seem over enthusiastic without adequate scientific rigor. One very recent publication with a larger number of MCS patients and longer follow-up showed that patients improved after stimulation therapy over a period of 16 months. In that article, the authors mentioned their selection criteria according to Jennett and Plum's definition in a systematized way and they reported display of emotional responses in patients [12]. In addition, clinical or electrophysiological responses were more visible after turning off the stimulation. In 2008, Liu showed in their study that SCS stimulation had to be continued for 290 days to recover the patient's consciousness. Conversely, stimulated their patients for 42 months in order to restore consciousness [12,13]. This long duration stimulation led to a proper carry-

over of observations and evaluations in both ON or OFF stimulation scenarios. In terms of neurophysiological, metabolic, and hemodynamic changes, neuro-stimulation showed enhancement of neurophysiological and EEG patterns as well as simultaneously showed improvement of metabolic patterns and amelioration of the CBF. In 2009, Liu demonstrated that SCS therapy improved CBF in the brain.

In this study, we have presented cases of 6 patients who recovered from MCS due to high cervical SCS therapy accompanied by electrophysiological evaluation to determine brain functionality. Of the multiple neuro-electrophysiological evaluations used, the ABR was used for finding brain stem functions, SEP for thalamo-cortical functions, and EEG helped us to compare the functionality between brainstem and cerebral cortex. Pain P250 systems were also used to analyze higher brain functionality [14]. All 6 patients met all selection criteria for HC-SCS and 6 out of 6 patients showed continuous functional improvements (such as differentiating between 2 objects and communicating with upper motor extremities) with stimulation, whereas at least 5 patients demonstrated improvement post switching off of the therapy after 12 months. Periodic BIS data monitoring and analysis throughout the stimulation period and beyond, which was not done in the previous studies, further helped establish the theory of the emergence of patients with HC-SCS therapy. This study also demonstrates that proper patient selection is very important, and that electrophysiological evaluations play a vital role in determining the outcome of the therapy [15].

Possible mechanisms: In their study, it is reported that in VS condition, patients have a combination of neuronal loss and neuronal dysfunctions [16]. The authors also reported that glucose metabolism in VS patients was approximately 50-70% of a normal person. Moreover, they suggested that loss of consciousness involved both physiological and anatomical factors [17]. The 'reticular formation-thalamus-cortex-pathway' hypothesis postulates that there is a connection between the ascending arousal system, the neuronal substrates of consciousness, and the coma. This theory is based on cortical functions, sleep-awake regulation and how the reticular formation influences the central thalamus and the cerebral cortex, which plays a critical role in maintaining the awake state [18,19]. From this, we assume that electrical stimulation can induce sufficient neural firing in most of these patients. In theoretical models, it has been demonstrated that an interaction exists between cortical pyramidal output neurons and reticular thalamic neurons [28]. Considering this hypothesis, we assume that SCS therapy modifies cortico-thalamic circuits and reticulo-cortico thalamic excitatory neurotransmission [29-32]. In the presence of an artificial excitatory device, the neocortical and striatal neurons which are connected to the reticular formation are likely to have significant network effects on the broad connectivity [27].

Conclusion

HC-SCS therapy shows significant improvements in patients with MCS. However, the successful emergence of patients from MCS by this therapy shall depend on the proper lead

placement and optimal programming of the SCS device. Therapy for chronic disorders of consciousness is a very protracted, long process with excessive expenses. This study provides evidence supporting improvement in MCS patients post SCS stimulation. We can hypothesize that high cervical stimulation in MCS patients induces clinical improvements by stimulation of the reticular formation thalamo-cortical pathway. High cervical stimulation therapy should thus be encouraged in further multicentre studies, with use of more specific patient selection on the basis of clinical and biochemical responses. We demonstrate that low frequency stimulation was associated with upper muscle twitches and high frequency stimulation was associated with increment of brain functional activities. The main criteria in proper patient selection should be by SPECT scan and rCBF value, as we have observed that patients with lower than 15 (ml/100 g/min) CBF value usually do not respond to HC-SCS. Thus, it is indeed possible to select the correct patient for HC-SCS therapy who has a high potential to emerge from the MCS state given proper anatomical position and programming sequences.

References

1. Bricolo A, Turazzi S, Faccioli F, et al. Clinical application of compressed spectral array in long-term EEG monitoring of comatose patients. *Electroencephalogr Clin Neurophysiol* 1978; 45(2):211-25.
2. Cohadon F, Richer E. Stimulation cérébrale profonde chez des patients en état végétatif posttraumatique : 25 observations. *Neurochirurgie* 1993;39(5):281-92.
3. Dempsey EWA, Morison RS. A study of thalamocortical relation. *Am J Physiol* 1942;135(2): 291-2.
4. Dieckmann G. Cortical synchronized and desynchronized responses evoked by stimulation of the putamen and pallidum in cats. *J Neurol Sci* 1968;7(2):385-91.
5. Fujii M, Sadamitsu D, Maekawa T, et al. Spinal cord stimulation therapy at an early stage for unresponsive patients with hypoxic encephalopathy. *No Shinkei Geka*, 1998;26(4):315-21.
6. Funahashi K, Komai N, Ogura M, et al. Effects and indications of spinal cord stimulation on the vegetative syndrome. *No Shinkei Geka* 1989;17(10):917-23.
7. Giacino JT, Ashwal S, Childs N, et al. The minimally conscious state: Definition and diagnostic criteria. *Neurology* 2002;58(3):349-53.
8. Hassler R, Ore GD, Dieckmann G, et al. Behavioural and EEG arousal induced by stimulation of unspecific projection systems in a patient with post-traumatic apallie syndrome. *Electroencephalogr Clin Neurophysiol*. 1969;27(3):306-10.
9. Hosobuchi Y. Electrical stimulation of the cervical spinal cord increase cerebral blood flow in humans. *Appl Neurophysiol.* 1985;48(1-6):372-6.
10. Jasper HH, Naquet R, King LE, et al. Thalamocortical recruiting responses in sensory receiving areas in the cat. *Electroencephalogr Clin Neurophysiol*. 1995;7(1):99-114.
11. Jennett B, Plum F. Persistent vegetative state after brain damage. *Lancet* 1972;299(7753):734-7.
12. Kanno T, Kamel Y, Yokoyama T, et al. Effects of dorsal column spinal cord stimulation (DCS) on reversibility of neuronal function-experience of treatment for vegetative states. *Pacing Clin Electrophysiol* 1989;12(4):733-8.
13. Kanno T, Morita I, Yamaguchi S, et al. Dorsal column stimulation in persistent vegetative state. *Neuromodulation* 2009;12(1):33-8.
14. Katayama Y, Tsubokawa T, Harano S, et al. Dissociation of subjective pain report and pain-related late positive component of cerebral evoked potentials in subjects with brain lesions. *Brain Res Bull* 1985;14(5):423-6.
15. Katayama Y, Tsubokawa T, Yamamoto T, et al. Characterization and modification of brain activity with deep brain stimulation in a persistent vegetative state: pain-related late positive component of cerebral evoked potential. *Pacing Clin Electrophysiol* 1991;14:116-21.
16. Liu JT, Tan WC, Liao WJ, et al. Effects of electrical cervical spinal cord stimulation on cerebral blood perfusion, cerebrospinal fluid catecholamine levels and oxidative stress in comatose patients. *Acta Neuro chir Suppl*, 2008;101:71-6.
17. Matsui T, Asano T, Takakura K, et al. Beneficial effects of cervical spinal cord stimulation (cSCS) on patients with impaired consciousness: a preliminary report. *Pacing Clin Electrophysiol* 1989;12(4):718-25.
18. Moruzzi G, Magoun HW. Brain stem reticular formation and activation of the EEG. *Electroencephalogr Clin Neurophysiol* 1948;1(1-4):455-73.
19. Ashwal S, Cranford R, Bernat JL, et al. Medical aspects of the persistent vegetative state. *N Engl J Med* 1994;330(21): 1499-508.
20. The Multi-Society Task Force on PVS: Medical aspects of the persistent vegetative state. *N Engl J Med*. 1994;330:1572-9.
21. Schiff ND, Giacino JT, Kalmar K, et al. Behavioural improvements with thalamic stimulation after severe traumatic brain injury. *Nature*. 2007;448(7153):600-3.
22. Sturm V, Kuhner A, Schmitt HP, et al. Chronic electrical stimulation of the thalamic unspecific activating system in a patient with coma due to midbrain and upper brain stem infarction. *Acta Neuro chir (Wien)* 1979;47(3):235-44.

23. Tsubokawa T, Yamamoto Y, Katayama Y, et al. Prediction of the outcome of prolonged coma caused by brain damage. *Brain Inj* 1990;4(4):329-37.
24. Tsubokawa T, Yamamoto Y, Katayama Y, et al. Deep brain stimulation in a persistent vegetative state: Follow-up results and criteria for selection of candidates. *Brain Inj*. 1990;4(4):315-27.
25. Yamamoto T. Response to Kanno et al.: Dorsal column stimulation in persistent vegetative state. *Neuromodulation* 2009;12(4):315.
26. Yamamoto T, Katayama Y. Deep brain stimulation therapy for the vegetative state. *Neuropsychol Rehabil* 2005;15:406-13.
27. Yamamoto T, Katayama Y, Kobayashi K, et al. DBS therapy for a persistent vegetative state: Ten years' follow-up results. *Acta Neuro chir Suppl* 2003;87:15-8.
28. Yamamoto T, Katayama Y, Kobayashi K, et al. DBS therapy for the vegetative state and minimally conscious state. *Acta Neuro chir Suppl* 2005;93:101-4.
29. Yamamoto T, Katayama Y, Kobayashi K, et al. Deep brain stimulation for the treatment of vegetative state. *Eur J Neurosci* 2010;32(7):1145-51.
30. Yamamoto T, Katayama Y, Obuchi T, et al. DBS and SCS for vegetative state and minimally conscious state. *World Neurosurg* 2013;80(3-4):1-9.
31. GM Della Pepa, C Fukaya, G La Rocca, et al. Neuromodulation of Vegetative State through Spinal Cord Stimulation: Where Are We Now and Where Are We Going? *Stereotact Funct Neurosurg* 2013;91(5):275-87.
32. Yamamoto T, Katayama Y, Obuchi T, et al. Spinal cord stimulation for treatment of patients in the minimally conscious state. *Neurol Me. Chir (Tokyo)* 2012;52(7):475–81.

***Corresponding to**

Pritam Majumdar

Department of Stereotactic and Functional Neurosurgery and Neuromodulation,

University Cologne Hospital,

Germany,

E-mail: drpritam.majumdar@neuraxisdb.com