# Breast cancer detection using modified Hough transform.

# Osama R. Shahin<sup>1,2\*</sup>, Meshrif Alruily<sup>3</sup>, Mansi Alsmarah<sup>1</sup>, Musharraf Alruwaill<sup>1</sup>

<sup>1</sup>Computer Science and Information Department, Faculty of Science & Arts, Jouf University, Saudi Arabia

<sup>2</sup>Physics and Mathematics Department, Faculty of Engineering, Helwan University, Egypt

<sup>3</sup>College of Computer and Information Sciences, Jouf University, Saudi Arabia

### Abstract

Breast cancer is a result of the uncontrolled cells division. These cells may spread from the breast to other parts of the body through blood vessels. Many symptoms were associated to the breast cancer, such as change in color, skin, and shape. In this work, the breast tumor will detect according to its geometric, texture, and gradient features. Firstly, region of interest (ROI) will detected by using the Hough transform. After the location of breast tumor was determined, these locations will cropping from the original mammogram image to detect the actual tumor, then twenty two features will be computed for the ROIs using predefined equations. These features are used to classify the infected tissues from the normal one. A comparison was made between system results of the breast features and reading of an expert's radiologist to ensure the feasibility and algorithm efficiency.

Keywords: Mammograms, Breast cancer, Hough transform.

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#### Introduction

Breast cancer is where anomalous cells develop in an uncontrolled manner. It is the most widely recognized reason for death among moderately aged ladies. The World Health Organization's International Agency for Research on Cancer in Lyon, France, has evaluated that in excess of million ladies overall kicked the bucket because of breast cancer every year [1].

Mammography helps in early location and it assumes a critical part in cancer treatment and permits a quicker recuperation for a large portion of the patients [2]. There are two sorts of mammography, film and computerized. Computerized mammography is superior to film mammography since radiation beams can be lessened up to half can even now identify breast cancer, while in film mammography the standard radiation beams can't be diminished [3,4]. Keeping in mind the end goal to enhance the biopsy yield proportion, masses must be named amiable or threatening.

Masses with sporadic in shapes are normally threatening, and those joined with radiolucent shapes are favourable [5,6]. In this work the digital mammogram images that were provided from online mammogram database (MIAS database) will be used [7]. Firstly, for each image the location for each suspicious areas will be decided and secondly a number of significant features-geometric, texture, and gradient features-will be computed [6,8-10].

### **Tumor Features**

There are a lot of features types that describe tumors in image. The function of features is to translate the medical statistics into decisions. Firstly, geometric features describe the geometric properties of the ROI. It is represented as a set of pixels in image [11,12]. Secondly, texture is really very fuzzy concept, these features of attempt to describe grayscale items between adjacent pixels in the image [13]. Finally, gradient is a subsidiary of the image among the neighbourhood respects. The Sobel operator is used to record gradient image as well [14].

### Methodology

The suspicious area (ROI) can be easily detected in a picture if the area contains enough background variation. The steps of the proposed can be summarized as follows:

### Reading the mammogram image

The images that are used in the algorithm from MIAS database [7], are firstly converted into gray level.

### Create gradient image

ROI differs significantly in contrast from the background. Changes in contrast can be detected by different operators such as Sobel, Prewitt, Roberts, Canny, etc. In this work, Sobel detector is used, due to its design simplicity.

# Subtracting the original image from the image after filling its gaps

After some of pre-processing process such as image dilates, fill interior gaps; the subtraction of the background from the filling images will be preceded. This process is very essential, to enhance the periphery of the ROI to make it easy to fit it in a circle that made in the following stage using Hough transform.

Feature	Equation			
Area meas- ure	$Area = \sum_{i} \sum_{j} (A_{i,j}, X_{ROI}(Area) = i, Y_{ROI}(Area) = j)$	(1)		
Perimeter	$Perimeter = \sum_{i} \sum_{j} (P_{i,j}, X_{edge}(Perimeter) = i, Y_{edge}(Perimeter) = j)$	(2)		
Compact- ness	$Compactness = \frac{p^2}{A}$	(3)		
Mean	$Compactness = \frac{P^2}{A}$ $Mean = \sum_{i=0}^{Arrec} Input Image[X_{ROI}(i), Y_{ROI}(i)]$	(4)		
Mean Global Area	$Mean\ Glopal = \sum_{i}^{NBL\ NBC} \sum_{i}^{NBL\ NBC} Input\ Image[i, j]$	(5)		
Mean Local Area	$Mean \ Local = \sum_{i}^{NBL} \sum_{j}^{NBL} Input \ Image[i, j]$	(6)		
Uniformity	$Uniformity = \sum_{i=0}^{Area} NH^{2}[Input Image[X_{ROI}(i), Y_{ROI}(i)]]$	(7)		
Standard Deviation	$SD = \sum_{i=0}^{N \times n} ([Input \ Image[X_{ROI}(i), Y_{ROI}(i)]] - Mean)^2$	(8)		
Smoothness	$Smothness = \frac{1}{1 + SD^2}$	(9)		
Skewness	$Skewness = \sum_{i=0}^{Arrea} ([Input \ Image[X_{ROI}(i), Y_{ROI}(i)]] - Mean)$	(10)		
Entropy	$Entropy = \sum_{i=0}^{Area} NH[Input Image[X_{ROI}(i), Y_{ROI}(i)])$	(11)		
Correlation	$\stackrel{i=0}{\longrightarrow} * logNH(Input Image[X_{ROI}(i), Y_{ROI}(i)])$ $Correlation = \sum_{i=0}^{Arrea} NH[Input Image[X_{ROI}(i), Y_{ROI}(i)])$ $* Input Image[X_{ROI}(i), Y_{ROI}(i)]$	(12)		
Inverse	$Inverse = \sum_{i=0}^{Arre} \left(\frac{1}{1 + (X_{ROI}(i) - Y_{ROI}(i))^2}\right) * NH(Input Image [X_{ROI}(i), Y_{ROI}(i)])$	(13)		
Sobal-Mean	$Sobal Mean = \sum_{i=0}^{Area} Gradient Image[X_{ROI}(i), Y_{ROI}(i)]$	(14)		
Sobal-Mean Global Area	Sobal Mean Glopal = $\sum_{i}^{NBL NBC} Sradient Image[i,j]$	(15)		
Sobal- Uniformity	$Sobal Uniformity = \sum_{i=0}^{Area} GBH^{2}[Gradient Image[X_{ROI}(i), Y_{ROI}(t)]]$	(16)		
Sobal- Standard Deviation:	$Sobal SD = \sum_{i=0}^{Area} ([Gradient \ Image[X_{ROI}(i), Y_{ROI}(i)]] - Mean)^2$	(17)		
Sobal- Smoothness:	$Sobal Smothness = \frac{1}{1 + Sobal SD^2}$	(18)		
Sobal- Skewness	$Slobal Skewness = \sum_{i=0}^{Area} ([Gradient Image[X_{ROI}(i), Y_{ROI}(i)]] - Mean)$	(19)		
Sobal- Entropy	$\sum_{i=0}^{Arrea} GNH[Gradient Image[X_{ROI}(i), Y_{ROI}(i)]) \\ * logPG(Gradient Image[X_{ROI}(i), Y_{ROI}(i)])$	(20)		
Sobal- Correlation	$ \begin{aligned} & \text{Sobal Correlation} = \\ & \sum_{i=0}^{lass} GNH[Gradient Image[X_{ROT}(i), Y_{ROT}(i)]) \\ & * Gradient Image[X_{ROT}(i), Y_{ROT}(i)] \end{aligned} $	(21)		
Sobal- Inverse	$\begin{split} & \text{Sobal Inverse} \\ & = \sum_{i=0}^{Area} \left( \frac{1}{(1 + (X_{ROI}(i) - Y_{ROI}(i))^2)} * \text{GNH}(\text{Gradient Image}\left[X_{ROI}(i), Y_{ROI}(i)\right]) \right) \end{split}$	(22)		
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Figure 1. List of tumor features.

### Detect the circular shape using the Hough transform

Hough transform is used here to surround the tumor area by a circle that closes to the surface dimension of the tumor [15]. The pseudo code of the algorithm can be summarized in Table 1.

Table 1. Pseudo	o code for	modified	Hough	transform.
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Load image
Find the edges in the image
For each edge point (xo, yo)
For (xo=xo_min; xo $\leq$ xo_max; xo++)

For (yo=yo_min; yo ≤ yo_max; yo++)
r=sqrt ((x-xo)^2+(y-yo)^2);
Accumulator (r) (xo) (yo)++; //Voting
Find the average values in accumulator for (r) (xo) (yo)

### Determine the features for the ROI

Here, the geometric, texture, and gradient features of ROI will be calculated using equations that predefined in [6,12,13]. Equations that needed to detect tumor features were listed in Figure 1.

## **Experimental Results**

This part introduces the experimental results of the proposed algorithm on the dataset consisting of 322 breast images from MIAS database that covering all cases of masses (malignant and benign) by different shapes, and size. The goal is to test and validate the proposed system presented in this paper in order to select the most suitable system. The total number of malignant samples that used here were 52, while the number for benign was 66 samples; finally normal samples were equal to 204. Table 2 lists the description of all images in the MIAS database and supplies the following significant information [16]. A portion of the tissues are darkened by a splendid area in the focal point of the mammogram. This brilliant locale makes the image be unevenly lit up.

Table 2. MIAS database description.

	Fatty tissues	Fatty glandular tissues	Dense tissues	Total		
Calcification	B:2	B:5	B:5	B:12	05	
Calcillon	M:4	M:4	M:5	M:13	25	
Circumscribed	B:7	B:6	B:3	B:16	- 20	
masses	M:2	M:2	M:0	M:4		
Spiculated masses	B:2	B:4	B:6	B:12	- 21	
opiculated masses	M:4	M:3	M:2	M:9		
Other, ill-defined	B:4	B:2	B:1	B:8	- 15	
masses	M:4	M:4	M:1	M:7	- 15	
Architectural	B:4	B:3	B:4	B:10	- 20	
distortion	M:2	M:4	M:4	M:10		
Asymmetry	B:2	B:3	B:3	B:8	- 17	
Asymmetry	M:3	M:2	M:4	M:9		
Normal	66	64	74	-	204	
Total	106	104	112	-	322	
B: Benign; M: Malignant.						

Because the background of the mammogram is dark and the image of tumor masses are lighter than the background of the

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image, the using of the top-hat transform is required to reduce uneven lighting. This transformation is defined as the difference between the original image and its opening. The opening of the image is the set of front parts of the image that fit a particular structural element. After the location of the tumor area from the entire breast locale the features for these district will be ascertained, as specified before; 22 features will be calculated and will be spared in database which contains 322 row, each row for one image and 22 features extraction that calculated based on equations (1-22). The terminology measurement, i.e. (performance criteria) of the work for system is shown in Table 3. After the location of breast cancer was determined by previous method, these locations will cropping from the original mammogram image to detect the actual tumor as depicted in Figure 2. As a result of breast tumor detection, a 22 features based upon the equations that explained in the methodology section will be calculate that shown in Table 4.

The results of the computed features by using the equations (2-23) appeared in Table 4. Based upon these features, the classification between the normal tissues and the other infected tissues can be determined by aiding of an expert radiologist.

The performance measures of the proposed algorithm with the other reliable classifiers are depicted in Table 5.

Table 3. Terminology measurement of	of the algorithm.
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TN	TP	FP	FN	Sensitivity (%)	Speci	ificity (%)	Accuracy (%)	Precision (%)	
164	136	16	6	95.77	90.9		93.17	89.47	
Table 4.	Feature ex	ctraction r	ange values	s for cancer tumor.		Author	Methodology		Acc.
Feature Maximum Minimum					ROIs are obtained using a proficient Otsu thresholding and then subjected to				
Area			260	75		Trbalić et al. [17]	processing stage. Then a collection of 32 Zernike		
Perimet	er		3580	270					
Compac	ctness		34.554	17.456			The regions of interest	(ROIs) are located by	
Mean			242.802	142.133	Liu et al. [18]		using multiple concentric l Then, ROIs are further re		I.
Mean gl	obal area		9.245	1.968			based active contour enhance the segmentation	· //	I.
Mean lo	cal area		13.176	1.858			A new CAD system depends on the maximur	he proposed system 95%~96	
Uniform	ity		4.993	1.177		learning machine (ELM). 1 Xie et al. [19] contains extraction fea			ature, selection of
SD			32.632	12.866			parameters, and rating areas containing tumor ma		70
Smooth	ness		0.006	0			The regions of interest (ROIs) can be dete		
Skewne	SS		37.466	-8.203		Proposed	via modified Hough tra features of this region by	means of predefined	
Entropy		-27.676	-197.477		equations described in paper, and comp with normal values with advice of radiological				
Correlat	ion		569	48			radiologist.		
Inverse			0.6446	0.001		100	Carl Zar	Path. F.	2
Sobal m	iean		97.459	44.597		6	- <b>166</b>	1000	
Sobal mean global		8.472	1.97		1. 1				
Sobal u	niformity		3.583	0.005		-4			-
Sobal S	D		27.639	5.948		100	100 100	ales 6	10
Sobal sr	moothness		0.0538	0.001		100	S) S		
Sobal sł	kewness		25.005	-5.538			1. The second		
Sobal er	ntropy		-20.214	-250.459		Figure 2. Tumor	detection by Hough tra	insform.	
Sobal co	orrelation		378	8		Conclusion			
Sobal in	verse		5.846	0.001		CUICIUSIUII			

*Table 5.* Performance comparison with the other reliable classifiers in terms of accuracy (Acc.).

From the comparison tests that for result shown in Table 5, we see that all features obtained by the proposed algorithm are matching with those features in the previous works. So, the proposed algorithm is able to detect the region of the tumors

and determine its locations. In addition to the last benefit it could detect more than one tumor in the same breast region which gives power to the proposed algorithm. As seen from the experimental results and from the performance comparison, the proposed features extraction shows a good result. Thus, it has an ability to implement such breast cancer detection system.

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# \*Correspondence to

Osama R. Shahin

Computer Science and Information Department

Faculty of Science & Arts

Jouf University

Saudi Arabia